Micro-CT in the Assessment of Pediatric Renal Osteodystrophy by Bone Histomorphometry

Renata C. Pereira,* David S. Bischoff,† Dean Yamaguchi,† Isidro B. Salusky,* and Katherine Wesseling-Perry*

Abstract

Background and objectives Computed tomography (CT) measurements can distinguish between cortical and trabecular bone density in vivo. High-resolution CTs assess both bone volume and density in the same compartment, thus potentially yielding information regarding bone mineralization as well. The relationship between bone histomorphometric parameters of skeletal mineralization and bone density from microcomputed tomography (μCT) measurements of bone cores from patients on dialysis has not been assessed.

Design, setting, participants, & measurements Bone cores from 68 patients with ESRD (age =13.9±0.5 years old; 50% men) and 14 controls (age =15.3±3.8 years old; 50% men) obtained as part of research protocols between 1983 and 2006 were analyzed by bone histomorphometry and μCT.

Results Bone histomorphometric diagnoses in the patients were normal to high bone turnover in 76%, adynamic bone in 13%, and osteomalacia in 11%. Bone formation rate did not correlate with any μCT determinations. Bone volume measurements were highly correlated between bone histomorphometry and μCT (bone volume/tissue volume between the two techniques: r=0.70; P<0.001, trabecular thickness and trabecular separation: r=0.71; P<0.001, and r=0.56; P<0.001, respectively). Osteoid accumulation as determined by bone histomorphometry correlated inversely with bone mineral density as assessed by μCT (osteoid thickness: r=-0.32; P=0.01 and osteoid volume: r=-0.28; P=0.05). By multivariable analysis, the combination of bone mineral density and bone volume (as assessed by μCT) along with parathyroid hormone and calcium levels accounted for 38% of the variability in osteoid volume (by histomorphometry).

Conclusions Measures of bone volume can be accurately assessed with μCT. Bone mineral density is lower in patients with excessive osteoid accumulation and higher in patients with adynamic, well mineralized bone. Thus, bone mineralization may be accurately assessed by μCT of bone biopsy cores. Additional studies are warranted to define the value of high-resolution CT in the prediction of bone mineralization in vivo.


Introduction

Bone disease (renal osteodystrophy) is a universal complication of advanced kidney disease, contributing to an increased fracture rate in adults (1) and fractures, bone deformities, bone pain, and growth failure in children (2). Because of the morbidity associated with bone disease, its assessment and treatment are of critical importance. Current guidelines recommend that bone turnover, mineralization, volume, strength, and growth be assessed in all adults and children with CKD, and the bone biopsy is the gold standard for the diagnosis of renal osteodystrophy (3,4). Because this is an invasive technique used primarily in the research setting, circulating biomarkers are often used to assess bone turnover, and estimates of bone volume and density are often obtained from imaging studies (5–7). To date, however, only one study has evaluated the relationship between imaging data and bone histomorphometry in patients on dialysis; in this study, differences in bone density, as assessed by in vivo quantitative computed tomography (QCT), were noted between adult patients on dialysis with high and low bone turnover (8). Since that time, newer microcomputed tomography (μCT) techniques have been developed that yield sensitive assessment of volume, trabecular volume, and density in bone samples. However, the correlation between histomorphometric parameters of bone turnover, mineralization, and computed tomography (CT) measurements of bone volume and density in bone cores from patients with advanced CKD remains unknown.

Thus, to assess the potential for μCT measurements to predict indices of skeletal mineralization in pediatric CKD, this study compared bone density parameters obtained by μCT scanning of bone biopsy cores with parameters of bone turnover, mineralization, and volume as assessed by bone histomorphometry.

Materials and Methods

Bone Cores

Transiliac bone biopsy cores obtained from pediatric patients with ESRD and control specimens from...
Table 1. Biochemical parameters in patients on dialysis with normal to high bone turnover, pure osteomalacia, and adynamic bone disease

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Dialysis: Normal to High Bone Turnover (n=52)</th>
<th>Dialysis: Pure Osteomalacia (n=7)</th>
<th>Dialysis: Adynamic Bone (n=9)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Calcium, mg/dl</td>
<td>9.4±0.1</td>
<td>7.7±1.1</td>
<td>8.9±1.1</td>
</tr>
<tr>
<td>Phosphorus, mg/dl</td>
<td>6.0±0.1</td>
<td>7.0±1.0</td>
<td>6.2±0.7</td>
</tr>
<tr>
<td>Alkaline phosphatase, IU/L</td>
<td>337±38</td>
<td>127±23b</td>
<td>538±145b</td>
</tr>
<tr>
<td>PTH (first generation IMA)</td>
<td>736 (422, 1063)</td>
<td>293 (289, 555)</td>
<td>45 (21, 220)c</td>
</tr>
</tbody>
</table>

Values are expressed as mean±SD, except PTH, which is expressed as median (interquartile range). PTH, parathyroid hormone; IMA, immunometric assay.

*p<0.01 between osteomalacia and normal to high bone turnover.

*p<0.04 between adynamic bone and osteomalacia.

*p<0.01 between adynamic bone and normal to high bone turnover.

Biochemical Values
Biochemical values were obtained at the time of bone biopsy. Serum calcium, phosphorous, and alkaline phosphatase concentrations were determined by a Technicon Autoanalyzer (17;27). The coefficients of variation for each of these metabolites have been previously published and are as follows: calcium: 1.3% (10); phosphorus: <1.5% (11); and alkaline phosphatase: <10% (12). Parathyroid hormone (PTH) levels were determined by the UCLA Clinical Laboratory using an immunometric PTH assay by Nichols (San Clemente, CA), which detects the full-length PTH molecule [PTH[1–84]] as well as C-terminal fragments of the PTH molecule up to and including PTH(7–84). The intra- and interassay coefficients of variation for this assay were 5.2% and 9.0%, respectively (13).

Histomorphometry
Five-millimeter-diameter specimens of iliac crest were dehydrated in alcohol, cleared with xylene, and embedded in methyl methacrylate before analysis. Static histomorphometric parameters were evaluated in undecalciﬁed 5-μm sections treated with Toluidine blue stain, and tetracycline labeling was assessed in unstained 10-μm sections.

Primary bone histomorphometric parameters were characterized in trabecular bone under ×200 magniﬁcation using the OsteoMetrics System (OsteoMetrics, Decatur, GA) by a histomorphometrist (R.C.P.). Mineralized bone was deﬁned by dark blue staining areas; pale-blue seams at least 1.5 μm in width were included in measurements of osteoid. Derived indices were calculated as described by Parmley et al. (14). Specimens were classiﬁed according to the Turnover, Mineralization, and Volume classiﬁcation system (4). Normal parameters of bone histomorphometry were deﬁned from bone biopsies obtained from a control group of 31 pediatric patients with normal kidney function (mean age, 12.4±8.4 years old; 71% boys; 48% white; 26% Hispanic) who were undergoing elective orthopedic surgery (9).

μCT Analyses
Bone samples were subjected to μCT analysis with the Scanco μCT™ (Scanco Medical AG, Bruttisellen, Switzerland) by an investigator (D.S.B.) blinded as to bone histologic diagnosis and biochemical parameters. Bones were oriented vertically in a 12.3-mm sample holder, and scans were performed using medium-resolution settings with a source voltage of 70 E (kVp) and I of 114 μA. The images had a ﬁnal element size of 12.5 μm. Two-dimensional images were analyzed using software supplied from Scanco Medical AG (Image Processing Language, version 5.6). Images were contoured to establish volumes of interest by visual examination of serial slices in all of the specimens. An optimum arbitrary threshold value of 230 (highlighting mineralized bone) was used uniformly for all specimens to quantify mineralized regions from surrounding unmineralized areas. Histomorphometric analysis of three-dimensional reconstructions was performed using Scanco Evaluation Script No. 5 (Bone Trabecular Morphometry) for three-dimensional image reconstruction and bone parameter determinations. Bone architecture measurements obtained included trabecular bone volume ratio (percentages), trabecular number (numbers per millimeter), trabecular thickness (micrometers), trabecular spacing (micrometers), connectivity (numbers per millimeter²), and trabecular and cortical bone mineral density (milligrams hydroxyapatite [HA] per centimeter³). Fourteen of the bone cores from which normal histomorphometric parameters were ascertained were of suitable quality for μCT and used as the normal control population for these measurements.

healthy individuals (9) were obtained from a deidentiﬁed repository maintained in the Division of Pediatric Nephrology at the University of California, Los Angeles (UCLA). Cores from patients on dialysis were obtained from research protocols performed at this institution between 1983 and 2006. Samples were chosen on the basis of bone histomorphometric diagnosis (vide infra): (1) normal to high bone turnover, (2) adynamic bone, and (3) osteomalacia. All study participants with ESRD had been treated with chronic cycling peritoneal dialysis before bone biopsy. No study participants had a history of metabolic bone disease other than renal osteodystrophy, none had undergone parathyroidectomy within the year preceding the biopsy, and none were treated with immunosuppressive therapy or recombinant human growth hormone within the year before the biopsy. Control cores were obtained from healthy children at the time of orthopedic surgery (9). All study participants had undergone double-tetracycline labeling before the bone biopsy. The study was approved by the Institutional Review Boards at UCLA and Veterans Affairs Sepulveda.
**Results**

**Sample and Patient Characteristics**

Bone cores from 68 patients with ESRD and 14 controls were analyzed by bone histomorphometry and μCT. The patients were normal or high bone turnover: 76%; adynamic bone disease: 13%; and osteomalacia: 11%. Biochemical values obtained at bone biopsy from 68 patients are displayed in Table 1.

**Bone Histomorphometry**

Consistent with previous pediatric data (15), bone volume (bone volume/tissue volume) and trabecular thickness were normal or increased, and values did not differ between histologic subtypes of renal osteodystrophy. By contrast and consistent with the definition of the different lesions, osteoid accumulation and bone turnover differed between groups. In patients in the normal to high bone turnover group, bone formation rate was normal in 23

**Statistical Analyses**

Variables are reported as means±SDs or medians (interquartile ranges). Pearson correlation coefficients were used to express the relationship between bone histomorphometric and μCT parameters; all parameters evaluated by this method had normal distributions. Multivariable linear regression was performed to assess the ability of μCT, biochemical measurements, and the presence or absence of vitamin D therapy at the time of bone biopsy to predict bone histomorphometric measures of unmineralized osteoid; skewed values (specifically PTH levels and bone formation rates) were log transformed to normalize their distribution before statistical analysis. All statistical analyses were performed using SAS software (SAS Institute Inc., Cary, NC), and all tests were two sided. A probability of type 1 error <5% was considered statistically significant, and ordinary P values are reported.

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Dialysis: Normal To High Bone Turnover (n=52)</th>
<th>Dialysis: Pure Osteomalacia (n=7)</th>
<th>Dialysis: Adynamic Bone (n=9)</th>
<th>Healthy Controls (n=14)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Bone volume (BV/TV), %</td>
<td>30.1±1.1</td>
<td>29.1±3.5</td>
<td>28.0±1.0</td>
<td>21.4±1.5</td>
</tr>
<tr>
<td>Trabecular thickness, μm</td>
<td>167±5</td>
<td>145±15</td>
<td>137±13</td>
<td>141±14</td>
</tr>
<tr>
<td>Trabecular separation, μm</td>
<td>406±16</td>
<td>343±38</td>
<td>355±29</td>
<td>459±22</td>
</tr>
<tr>
<td>Osteoid volume (OV/BV), %</td>
<td>11.9±0.7</td>
<td>28.4±3.9</td>
<td>1.1±0.4&lt;sup&gt;a&lt;/sup&gt;</td>
<td>2.2±0.4</td>
</tr>
<tr>
<td>Osteoid surface (OS/BS), %</td>
<td>47.0±1.8</td>
<td>67.2±6.5</td>
<td>10.0±2.0&lt;sup&gt;a&lt;/sup&gt;</td>
<td>16.6±2.7</td>
</tr>
<tr>
<td>Osteoid thickness, μm</td>
<td>19.8±0.6</td>
<td>27.8±4.0</td>
<td>6.1±0.6&lt;sup&gt;a&lt;/sup&gt;</td>
<td>8.3±0.8</td>
</tr>
<tr>
<td>Bone formation rate (BFR/BS), μm&lt;sup&gt;3&lt;/sup&gt; / μm&lt;sup&gt;2&lt;/sup&gt; per year</td>
<td>85.2 (51.7, 133.4)</td>
<td>0 (0, 7.7)</td>
<td>0.8 (0, 5.9)</td>
<td>59.1 (23.0, 64.7)</td>
</tr>
</tbody>
</table>

BV/TV, bone volume/tissue volume; OV/BV, osteoid volume/bone volume; OS/BS, osteoid surface/bone surface; BFR/BS, bone formation rate/bone surface.

<sup>a</sup>P<0.001 between adynamic bone and osteomalacia for OV/BV, OS/BS, and osteoid thickness.

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**Table 2.** Bone histomorphometric parameters in patients on dialysis with normal to high bone turnover, pure osteomalacia, and adynamic bone disease and healthy controls

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Dialysis: Normal To High Bone Turnover (n=52)</th>
<th>Dialysis: Pure Osteomalacia (n=7)</th>
<th>Dialysis: Adynamic Bone (n=9)</th>
<th>Healthy Controls (n=14)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Bone volume (BV/TV), %</td>
<td>32±1</td>
<td>23±3</td>
<td>29±2&lt;sup&gt;a&lt;/sup&gt;</td>
<td>20±2</td>
</tr>
<tr>
<td>Connectivity density, no. per millimeter&lt;sup&gt;2&lt;/sup&gt;</td>
<td>17.4±1.2</td>
<td>36.3±13.4</td>
<td>21.3±2.7&lt;sup&gt;a&lt;/sup&gt;</td>
<td>16.5±2.2</td>
</tr>
<tr>
<td>Trabecular no., no. per millimeter</td>
<td>2.0±0.1</td>
<td>2.3±0.2</td>
<td>2.1±0.1</td>
<td>1.8±0.1</td>
</tr>
<tr>
<td>Trabecular thickness, μm</td>
<td>160±10</td>
<td>120±10</td>
<td>150±10</td>
<td>140±10</td>
</tr>
<tr>
<td>Trabecular separation, μm</td>
<td>500±20</td>
<td>480±50</td>
<td>460±40</td>
<td>550±30</td>
</tr>
<tr>
<td>Bone mineral density, mg HA/cm</td>
<td>814±7</td>
<td>784±15</td>
<td>821±8&lt;sup&gt;a&lt;/sup&gt;</td>
<td>792±9</td>
</tr>
</tbody>
</table>

BV/TV, bone volume/tissue volume; HA, hydroxyapatite.

<sup>a</sup>P=0.03 between adynamic bone and osteomalacia for both bone volume and bone mineral density.
individuals and increased in 29 individuals, whereas osteoid volume was increased from the normal range in the majority. Osteoid volume was further increased in patients with osteomalacia, although bone formation was suppressed in these individuals. By contrast, both bone turnover and osteoid accumulation were decreased in patients with adynamic bone. By definition, osteoid accumulation as assessed by bone histomorphometry was higher in patients with osteomalacia than in those with adynamic bone ($P<0.001$ between groups) (Table 2).

As previously described (15), serum PTH and alkaline phosphatase values correlated directly with bone formation rate ($r=0.67$; $P<0.001$ and $r=0.38$; $P=0.004$ for PTH and alkaline phosphatase, respectively) as well as with osteoid accumulation (osteoid thickness: $r=0.54$; $P<0.001$ and $r=0.34$; $P<0.01$, respectively), whereas serum calcium levels were inversely related to osteoid thickness ($r=-0.43$; $P<0.001$).

$\mu$CT Parameters and Their Relationship to Biochemical Parameters and Bone Histomorphometry

In contrast to histomorphometric measurements, $\mu$CT measurements of bone volume differed between histologic subgroups, with bone volume appearing lower in patients with osteomalacia than in those with adynamic bone disease ($P=0.03$ between groups). $\mu$CT measurements of bone mineral density also appeared lower in patients with osteomalacia than in those with adynamic bone ($P=0.03$ between groups) (Table 3), and values were inversely correlated with both serum PTH levels ($r=-0.35$; $P<0.01$) and alkaline phosphatase activity ($r=-0.57$; $P<0.001$).

Although histomorphometric measurements of bone formation rate did not correlate with any $\mu$CT determinations, bone volume measurements were correlated between bone histomorphometry and $\mu$CT. The correlation coefficient between bone volume/tissue volume as assessed by the two techniques was $r=0.70$ ($P<0.001$) (Figure 1), whereas the correlation between measurements of trabecular thickness and trabecular separation were $r=0.71$ ($P<0.001$) (Figure 2) and $r=0.56$ ($P<0.001$) (Figure 3), respectively. Although the accumulation of unmineralized osteoid was not directly assessed by $\mu$CT, bone mineral density as assessed by $\mu$CT correlated inversely with osteoid accumulation as determined by bone histomorphometry ($r=-0.32$; $P=0.01$) (Figure 4) and osteoid volume/bone volume ($r=-0.28$; $P=0.05$). Correcting by $\mu$CT measures of bone volume bone mineral density predicted histomorphometric measurements of bone osteoid volume with an adjusted $R^2$ of 0.15 ($P=0.003$). The addition of PTH and calcium to the model further improved the prediction of osteoid volume to a final adjusted $R^2$ of 0.38. Considering whether the study participant was receiving vitamin D therapy at the time of bone biopsy did not change the predictive capability of this model.

Discussion

Assessment of bone turnover, mineralization, and volume is recommended for the diagnosis of the different subtypes of renal osteodystrophy in CKD (3,4), because all parameters likely contribute to bone fragility, deformities, and/or poor growth. Currently, the gold standard for the assessment of all three parameters continues to be the bone biopsy; however, to avoid the invasive nature of the bone biopsy, noninvasive techniques, such as pQCT, QCT, and dual-energy x-ray absorptiometry (DXA), are widely used for the evaluation of bone mass/bone volume. These techniques are not equivalent, because the predictive capability for bone volume varies markedly between techniques, and none to date have been evaluated in their ability to assess skeletal mineralization using bone histomorphometry as a standard. This study, in which bone histomorphometric measures of osteoid accumulation correlated with $\mu$CT measures of bone mineral density, suggests that skeletal mineralization, in addition to bone volume, may be assessable by high-resolution bone CT in bone cores from patients on dialysis.

Various investigators have evaluated the ability of imaging techniques to predict both bone composition and structure. Wehrli et al. (16) have performed many studies on the value of magnetic resonance imaging...
(MRI) in the assessment of bone mineralization in animals, with mineralization assessed by multiple techniques, including ash weight, 31P solution nuclear magnetic resonance, CT density, and water content. Wehrl et al. (16) have also evaluated the potential clinical use of MRI in 17 pediatric patients on dialysis (16); however, no comparison with histomorphometry was performed in this analysis, and assessment was limited to bone volume and structure. Misoff et al. (17) also evaluated the relationship between cortical and cancellous mineralization parameters by backscatter electron microscopy in adults with normal kidney function; however, histomorphometric variables were likewise not reported in this analysis. Two studies in individuals with normal kidney function—one by Borah et al. (18) and one by Tamminen et al. (19)—did relate imaging measures to bone histomorphometry. Borah et al. (18) showed an improvement in the proportion of highly mineralized bone as assessed by μCT in adults in response to bisphosphonate therapy—an improvement that correlated with changes in bone formation ($R^2=0.79$), and Tamminen et al. (19) showed that mineralization heterogeneity, as determined by backscatter electron microscopy, correlated with histomorphometric parameters and serum markers of bone turnover in pediatric patients with osteoporosis. Boling et al. (8) have also previously shown that bone density, as assessed by QCT, differed between adult patients on hemodialysis with low and high bone turnover. However, in each of these previous studies, it is important to consider that assessment of skeletal mineralization, independent of bone turnover, was not considered, and although bone turnover and skeletal mineralization tend to be highly correlated in individuals with normal kidney function, defects in skeletal mineralization may be independent of altered bone turnover in the pediatric CKD population (20–22).

A variety of biomarkers, including calcium, phosphorus, alkaline phosphatase, and PTH values, have all been used to assess bone quality in the pediatric CKD population. Despite much research and innovations in assay techniques over the years, however, these tests remain imperfect in their assessment capability. Current Kidney Disease Improving Global Outcomes guidelines suggest that PTH values within a very wide range (two to nine times the normal range) are associated with normal bone turnover, and current pediatric guidelines vary considerably according to region (Kidney Disease Outcomes Quality Initiative and European guidelines). Over the past decade, reassessment of biomarkers has suggested that the use of a combination of serum calcium, PTH, and alkaline phosphatase may aid the assessment of both bone turnover and skeletal mineralization and that a new biomarker, fibroblast growth factor 23, may predict skeletal mineralization. Although bone histomorphometry remains the gold standard for the assessment of bone turnover, mineralization, and volume in CKD, this analysis suggests that the addition of biochemical parameters to noninvasive imaging analysis improves the assessment of skeletal mineralization in pediatric patients with ESRD. Although this finding is promising, an $R^2$ of 0.38 for the model as a whole—including μCT measures of bone volume, bone mineralization, serum calcium, and serum PTH levels—suggests that these factors together predict 38% of the variation in osteoid volume, leaving another 62% of the variation unrelated to these factors. Dialysis vintage may also affect bone structure and composition, and certain treatments, including vitamin D sterols (21) and growth hormone therapy (23), have been shown to disrupt the relationship between bone turnover and PTH. In this study of patients who were relatively new to dialysis, the addition of the presence of active vitamin D sterol therapy to the model did not improve prediction of osteoid accumulation. Circulating values of fibroblast growth factor 23 have also previously been associated with indices of skeletal mineralization in the pediatric dialysis population (20,24), and other markers of bone health, including circulating sclerostin levels and 25(OH) vitamin D stores, may affect skeletal mineralization; whether the addition of these

Figure 3. Correlation between trabecular separation measurements. Pearson correlation between measurements of trabecular separation (Tb.Sp) as assessed by bone histomorphometry versus microcomputed tomography (μCT).

Figure 4. Correlation between bone mineral density and osteoid accumulation. Pearson correlation between measurements of unmineralized osteoid accumulation (osteoid thickness [O.Th]) as assessed by bone histomorphometry and bone mineral density as assessed by microcomputed tomography (μCT). HA, hydroxyapatite.
parameters to traditional biochemical markers and μCT measurements can aid in the assessment of skeletal mineralization in the CKD population as a whole remains unknown.

This study consisted of a comparison between parameters of bone as assessed by bone histology and μCT measurements of bone biopsy specimens. Differences were noted within patients with respect to the amount of osteoid accumulation; however, future prospective studies are needed to assess the power of μCT in discriminating between normally and abnormally mineralized bone. It is also important to note that the μCT measurements in this study were obtained from bone biopsy specimens. Whether measurements obtained by μCT measurements directly in patients will yield similar results and whether measurements of bone density and structure at other sites will be related to bone histomorphometric parameters as assessed in the iliac crest are currently unknown. The benefit of CT scanning, relative to other imaging techniques, also remains an open question. Indeed, the use of CT scans—particularly on a repeated basis—in children is not without risk; cumulative doses of 50 mGy might almost triple the risk of leukemia, and doses of about 60 mGy might triple the risk of brain cancer (25). Other techniques, such as MRI, have no ionizing radiation; however, the relative ability of these two techniques to assess skeletal mineralization in bone cores, let alone in patients themselves, is unknown and warrants study.

In conclusion, these data confirm that measures of bone volume can be accurately assessed with μCT. Skeletal mineralization may also be assessed by μCT of bone biopsy cores, because bone mineral density was determined to be lower in patients with extensive osteoid accumulation and similar amounts of bone volume and higher in patients with adynamic, well mineralized bone. The potential value for noninvasive high-resolution CT assessment of bone in vivo to predict mineralization is unknown and warrants additional investigation.

Acknowledgments

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Disclosures

None.

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